

Fall Cushion for Hip Fracture Prevention

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INTRODUCTION

Background:

- 54 million older Americans (65+) are currently at risk of intertrochanteric hip fractures (IHF) resulting from a fall¹
- 300,000 older individuals are hospitalized each year for hip fractures²
- IHF causes a \$2.63 billion economic burden on the American healthcare system¹



Intertrochanteric hip fracture⁵

Problem / Gap:

- Devices that prevent fall injuries like grab bars and fall mats are dependent on location
- Wearable fall injury prevention devices like TangoBelt³ and Hip'Guard⁴ can be noticeable, expensive, and uncomfortable



Needs statement:

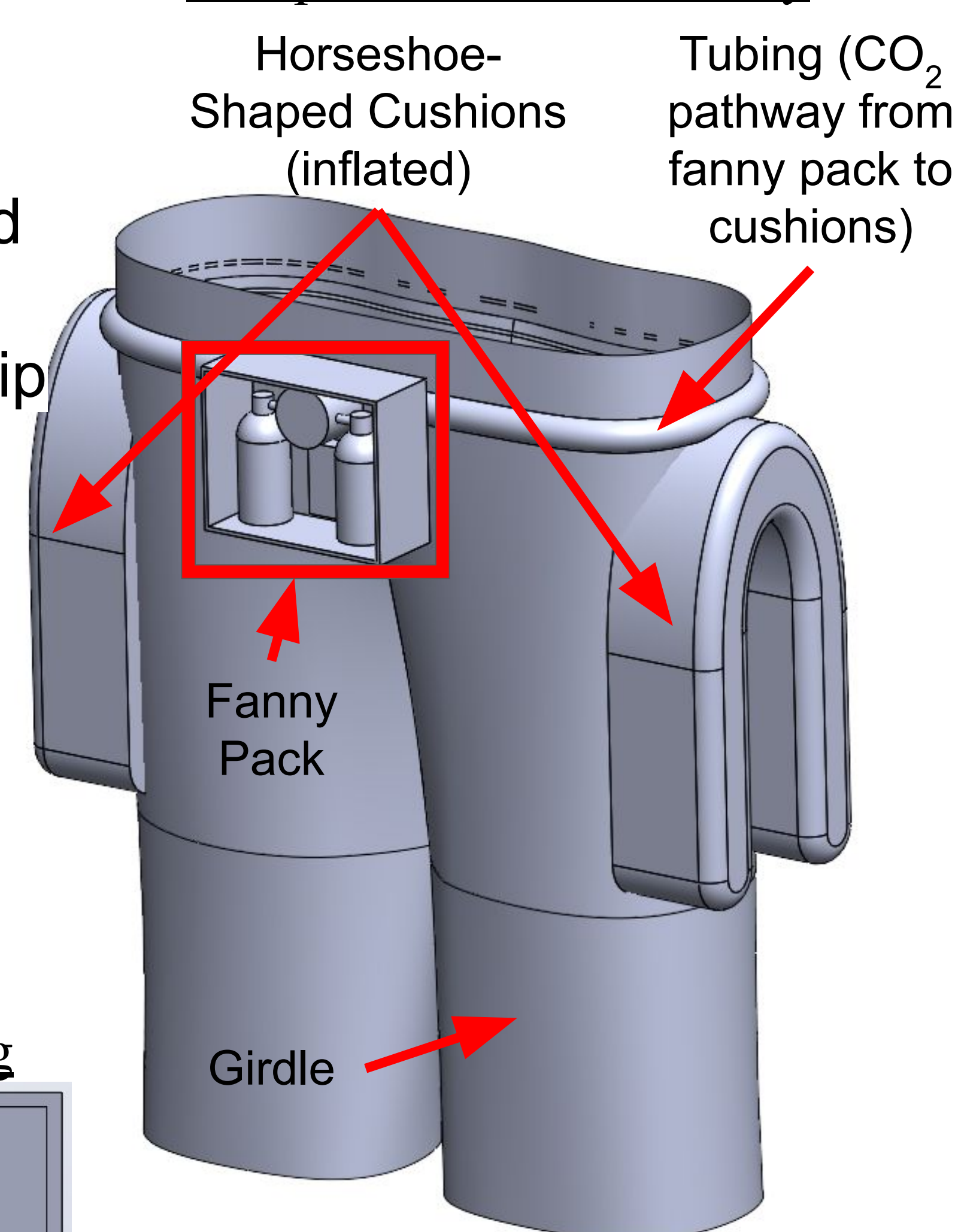
To reduce occurrence and injury extent of **hip fractures** among those who are at **risk of falling**, particularly in the **elderly community**, by creating a comfortable, unobtrusive **fall cushion** that is affordable, aesthetically pleasing, and user-friendly.

PROPOSED SOLUTION

Final Design:

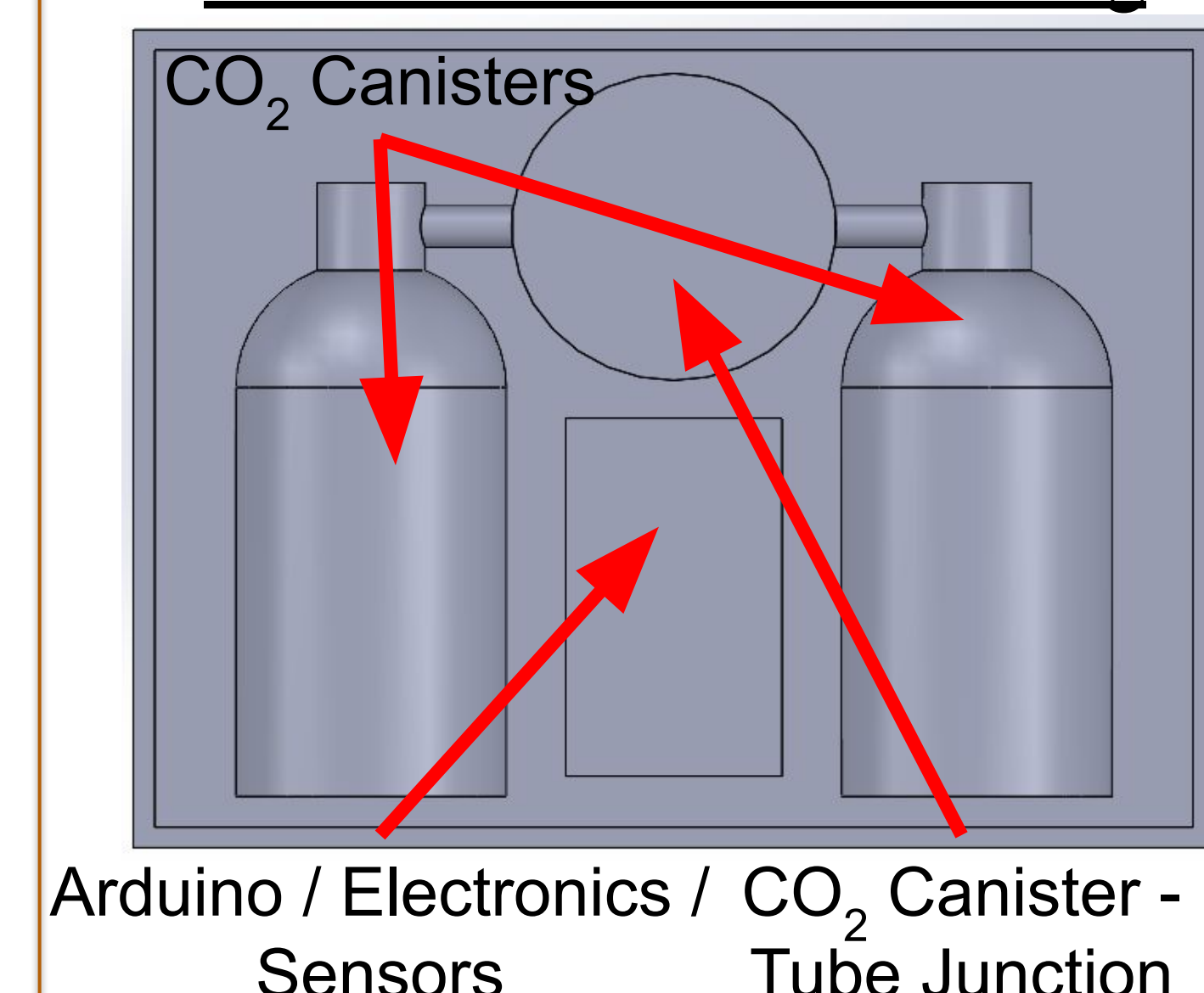
- Discreet undergarment with attached inflatable airbags
- Nylon horseshoe-shaped cushion for maximum diversion of force from hip joint
- Fanny pack containing canisters, electronics and gyroscope / accelerometer sensors
- Reusable & washable girdle

Figure 1: CAD Model of Complete Device Assembly



- Fall-detection algorithm signals a solenoid valve to open
- Canisters with compressed CO₂ release gas through tubing into the airbag cushions

Figure 2: CAD Model of Device's Electronics Housing



INFLATABLE CUSHION TESTING

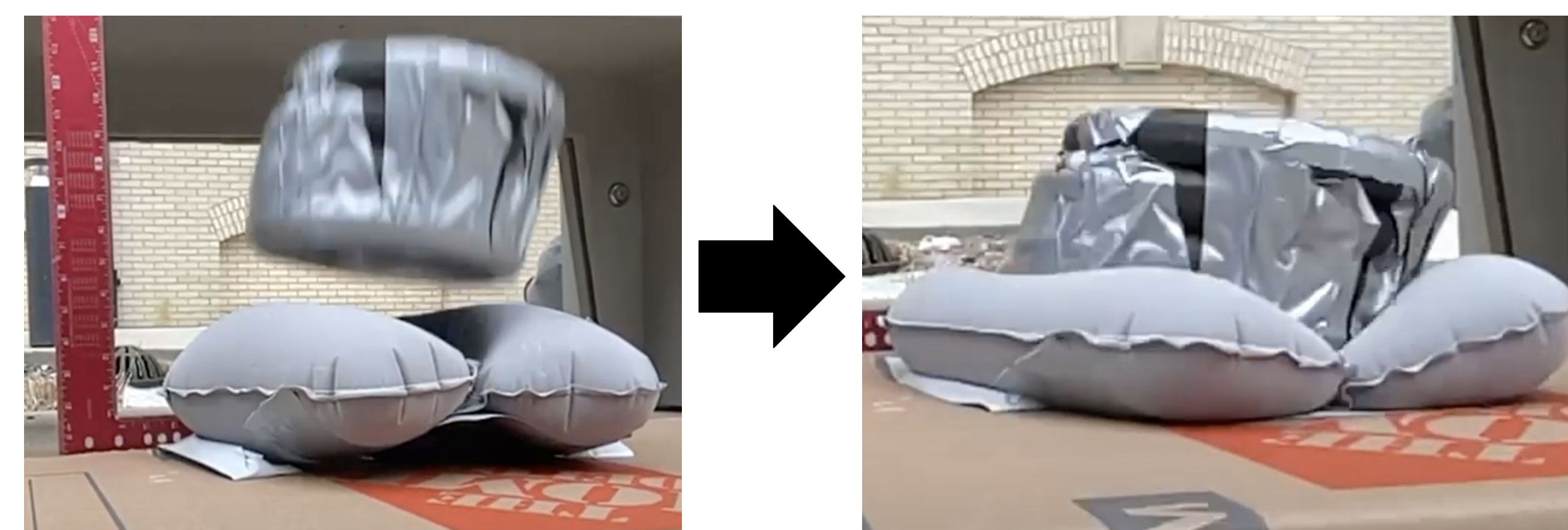
Pressure Testing:

- Used a manometer while the CO₂ canister discharges to measure the pressure while the device is inflated
 - Pressure range reached in cushion: 1.1-1.4 PSI

Impact Testing:

$$\text{Impact Force} = \frac{\text{mass} * \text{gravity acceleration} * \text{height}}{\text{distance traveled}}$$

- Used the force work equation to calculate that a 45lb plate dropped at 0.7m produces a 5200N impulse
 - 5200N is the median value of the femoral force in an unexpected sideways fall for an average person⁷



- 2.39 in avg. cushion compression at operating pressure
 - Cushion did not leak or lose air pressure after 6 consecutive trials
 - Cushion did not pop after pressure and impact testing

Table 1: Average Compression of the Hip Analog (Silly Putty Ball) With and Without Air Cushion Present

Test Group	Mean Compression of Silly Putty (in)
Control (without cushion)	1.25 ± 0.90
Experimental (with cushion)	0.39 ± 0.15

GENERAL FEASIBILITY

Cost:

- Manufacturing costs estimated at about \$87.15/unit
- Cost to customers is predicted to be less than \$200
 - Hip'Guard priced at \$800⁴
 - TangoBelt priced at \$1500³

Table 2: Cost to Produce 100k Devices Annually (per unit)

Components	\$87.15
Assembly (labor)	\$20.00
Quality Assurance and Testing	\$5.00
Total	\$112.15

Reimbursement:

- Fall prevention devices (both our device and our competitors) are not listed on the covered medical devices list from the Centers for Medicare and Medicaid Services⁸

Patentability:

- US Patent US5500952A is a "Hip Inflation Protection Device" we believe resembles our project⁹
- Key differences between this device and our own include that our device is **not a belt** and does not include a pleated, folded cushion that expands

ACKNOWLEDGEMENTS

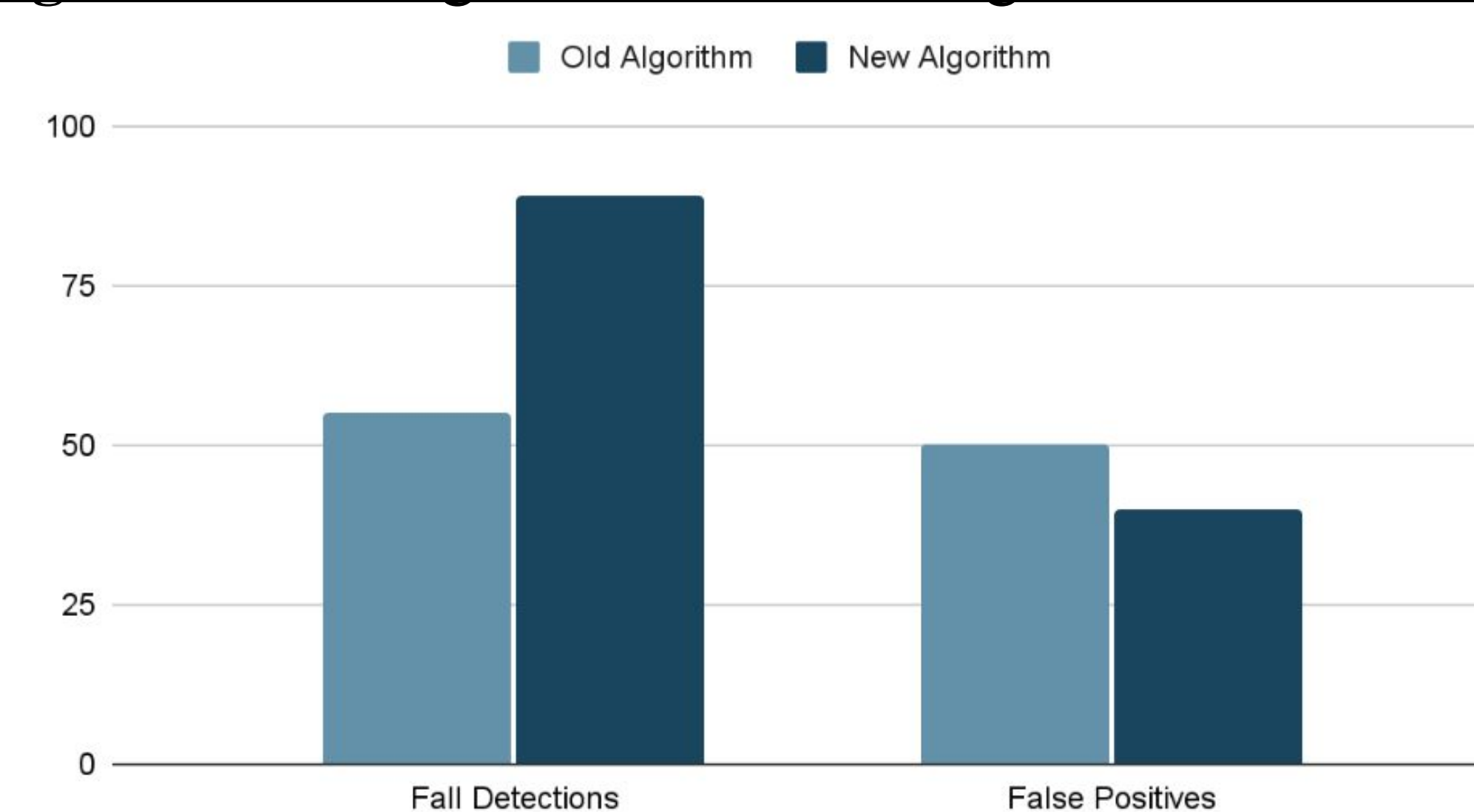
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ELECTRONICS & LATENCY TESTING

Accurate Fall Detection Testing:

- How often does the algorithm detect a fall correctly?
 - The current fall detection algorithm can detect falls accurately, 80% of the time (16 times out of 20 trials)

Figure 3: Old Algorithm vs. New Algorithm Performance



Latency Testing:

- Due to limitations in junction strength, latency from detection to inflation had to be estimated
- Once air valve was opened, the cushions inflated within 2-3 seconds
- Once a fall is detected, the algorithm takes approximately 5 milliseconds to send the signal to the solenoid
 - Response is limited by the baud rate of 9600ms for the microcontroller

REFERENCES

1. Adeyemi, A., & Delhougne, G. (2019). Incidence and Economic Burden of Intertrochanteric Fracture. *JBS Open Access*, 4(1), e0045. <https://doi.org/10.2106/jbjs.oe.18.00045>
2. Centers for Disease Control and Prevention. (2017, February 10). Important facts about falls. Centers for Disease Control and Prevention. Retrieved September 29, 2021, from <https://www.cdc.gov/homeandrecreationsafety/falls/adultfalls.html>.
3. Tango® belt - hip protection redefined. Tango® Belt - Hip Protection Redefined. (n.d.). Retrieved October 8, 2021, from <https://www.tangobelt.com/>.
4. "The Airbag Belt for Seniors That Protects the Hips." Hip Guard, 4 May 2021, <https://hipguard.eu/en/>.
5. "Hip Fractures - OrthoInfo - Aaos." OrthoInfo, <https://orthoinfo.aaos.org/en/diseases--conditions/hip-fractures>.
6. Straight Grab Bar - 18. (2010). ULINe. https://www.uline.com/Product/Detail/H-6483/Bathroom-Supplies/Straight-Grab-Bar-18?picode=WB0036&gadtype=pla&id=H-6483&gclid=Cj0KCQjw37ITBhCWARIsACBt1lwc5GKqSKGrPQTWuyy3_RBtr7ec2aMUU-q89HvyINsd4VCfvrH1fv0aAvz0EALw_wcB&gclid=aw.ds
7. Nasiri Sarvi, M., & Luo, Y. (2017). Sideways fall-induced impact force and its effect on hip fracture risk: a review. *Osteoporosis International*, 28(10), 2759–2780. <https://doi.org/10.1007/s00198-017-4138-5>
8. Medicare.gov. (2020). Medicare. <https://www.medicare.gov/Pubs/pdf/11045-medicare-coverage-of-dme>
9. Keyes, M. J. (1994b, October 28). Hip inflatable protection device. Google Patents. Retrieved February 18, 2022, from <https://patents.google.com/patent/US5500952A/en>.